

# Development of a Novel Pediatric Forearm Fracture Treatment: Simulation, Prototype and Evaluation

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## Background

Distal forearm fractures (DFF) are among the most common childhood injuries with current treatments split between conservative casting with closed reduction, and surgical techniques, for larger displacements [1, 2]. A treatment gap exists for moderately displaced DFF, which are associated with a higher rate of improper reduction when treated conservatively [2]. The fracture therapy presented in this study aims to fill this gap by introducing a novel reduction method without the need for invasive surgery [3].

## Novel Fracture Treatment

A hinged cast system, with adjustable external angulation, counteracts the initial fracture angle to maintain a successful fracture reduction. The mechanical behavior is achieved via a cast attachment, positioned between the padding and casting material of the forearm cast (Fig. 1). Three hooks transfer an external tension to the cast, causing a hinge-like rotation (Fig. 2).

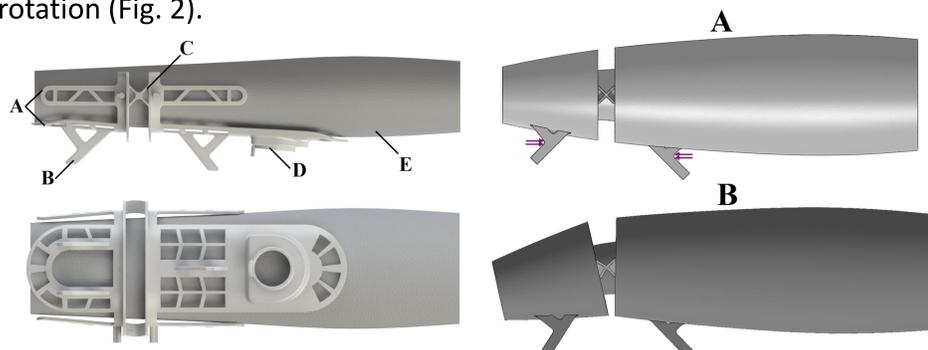


Fig. 1- Cast attachment placed over padding : (A) main body, (B) guide hooks, (C) truss joint, (D) dial mount (E) cast padding.

Fig. 2- Mechanical behavior of system: (A) before and (B) after the external load is applied (purple vectors).

## Prototype

- CAD simulation revealed design changes needed for improved integration of cast attachment and prevention of material failure
- Redefined geometry reflects pediatric forearm anatomy and reduces stress concentration in truss joint
- Biomechanical pediatric forearm phantom developed for prototype (Fig. 5): cast silicone-based phantom with embedded 3D-printed bone models simulates both-bone complete DFF with 15° fracture angle [4]
- Boa closure system ([www.theboasystem.com](http://www.theboasystem.com)) applies external load



Fig. 5- Assembled prototype of cast system. The forearm phantom is covered with a cotton cast sleeve and the redesigned cast attachment (3D-printed from polyamide 12) is placed over the sleeve. Synthetic casting material secures the cast attachment to the forearm.

## Biomechanical Simulation

- Age-specific CAD model of pediatric forearm and cast system (Fig. 3)
- Each component defined by modulus of elasticity, Poisson's ratio, and density [4]
- Discretized with solid, tetrahedral mesh (element size 1.0-5.0 mm)
- Linear static FEA for applied loads of 25 - 100 N
- Angular displacements calculated to derive external versus internal angulation of the system (Fig. 4) and max. von Mises stress examined for potential material failure [5]

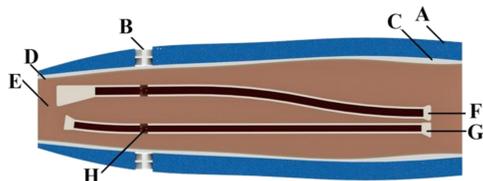


Fig. 3- Cross-section of CAD forearm model and cast system: (A) casting material, (B) imbedded cast attachment, (C) padding, (D) skin, (E) soft tissue, (F) radius, (G) ulna, (H) fracture site (hinge-joint).

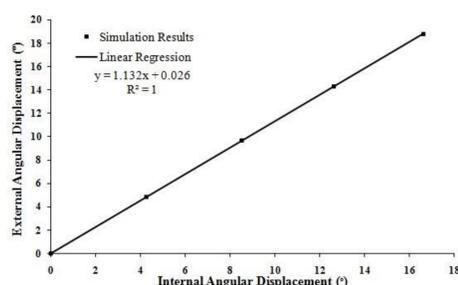


Fig. 4- External versus internal angular displacement. Markers show simulation values and derived linear regression with an  $R^2$  value of 1.

## Evaluation and Results

- Testing and radiographic imaging of prototype performed in the Department of Pediatric Surgery, UKSH, Lübeck Campus
- Lateral radiographs of system before and after reduction (Fig. 6)

Table 1: Summary of lateral radiographs describes the measured angle, calculated fracture angle, and external cast angle before and after manipulation.

	Measured Internal	Calculated Internal	Cast Angle
Initial	165.06°	14.94°	0°
Manipulated	179.81°	0.19°	16.57°

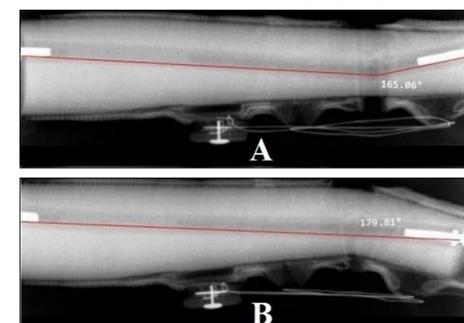


Fig. 6- Lateral view of cast system (A) before and (B) after manipulation.

## Conclusion and Future Work

Results of the study support the capability of the novel treatment to reduce a 15° initial fracture to < 1° of residual angulation. Future models should consider various muscle states to evaluate total treatment scope.

## References

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